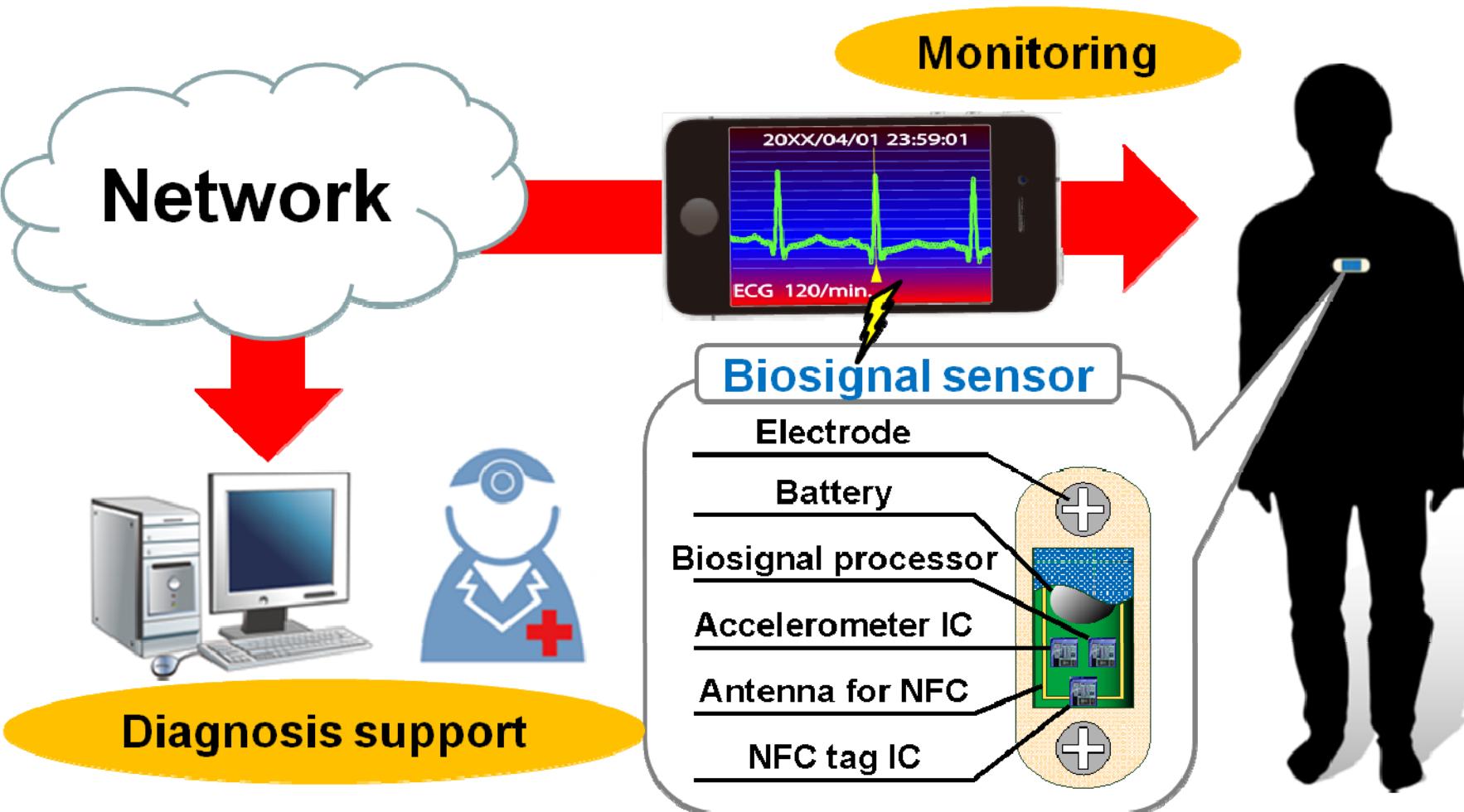


Normally-Off Technologies for Healthcare Appliance

*Shintaro Izumi¹, Hiroshi Kawaguchi¹, Yoshikazu Fujimori²,
and Masahiko Yoshimoto¹*

¹Kobe University, Kobe, Japan, ²Rohm, Kyoto, Japan

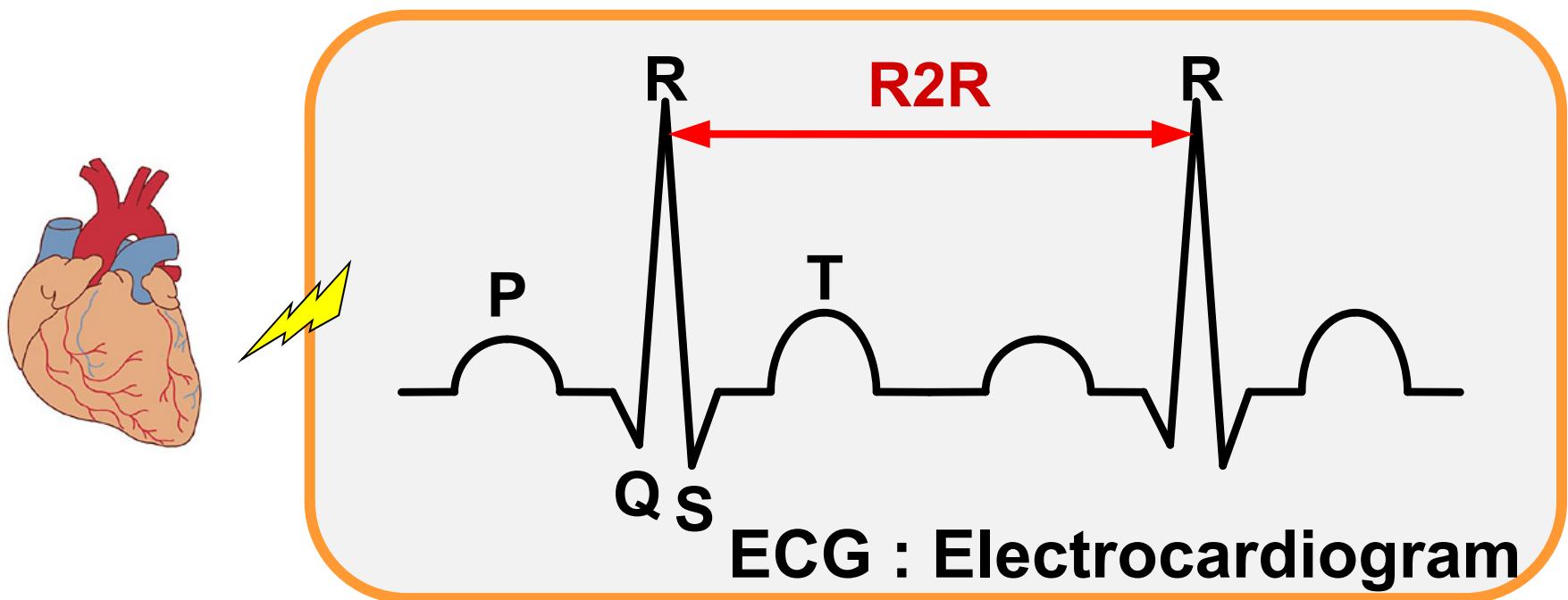
Wearable Healthcare System



Proposed LSI: IHR monitor

IHR (Instantaneous Heart Rate)

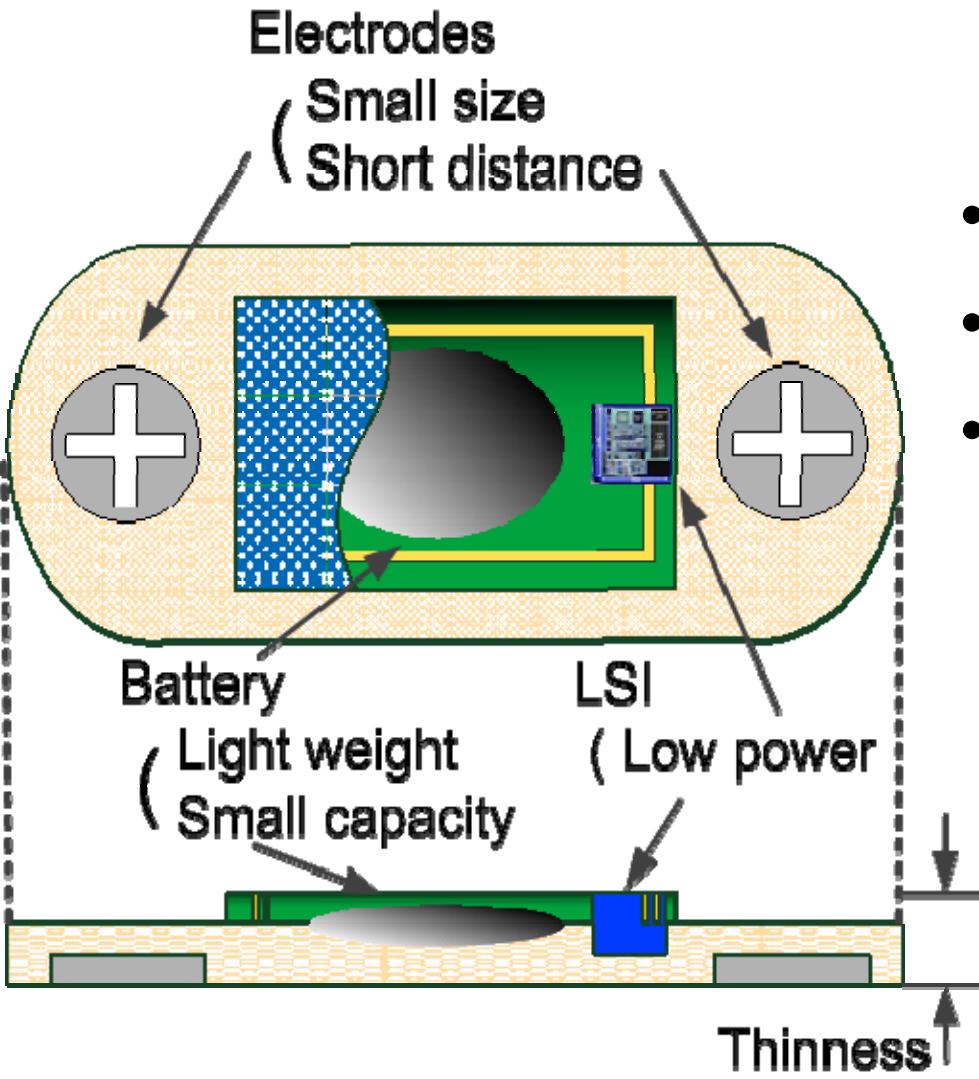
$$= 60 / (\text{newest R2R interval [s]}) [\text{bpm}]$$



Applications :

- ✓ Heart Rate Variability (HRV) analysis
- ✓ Exercise intensity estimation

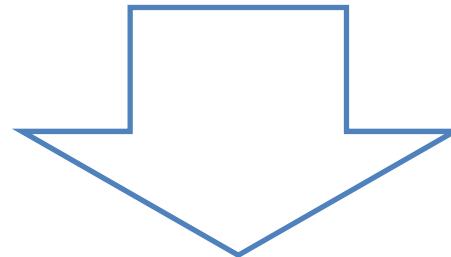
Constraints of Wearable Sensor



Requirement

- Small size
- Light weight
- Low cost

✓ Electrode
✓ Battery

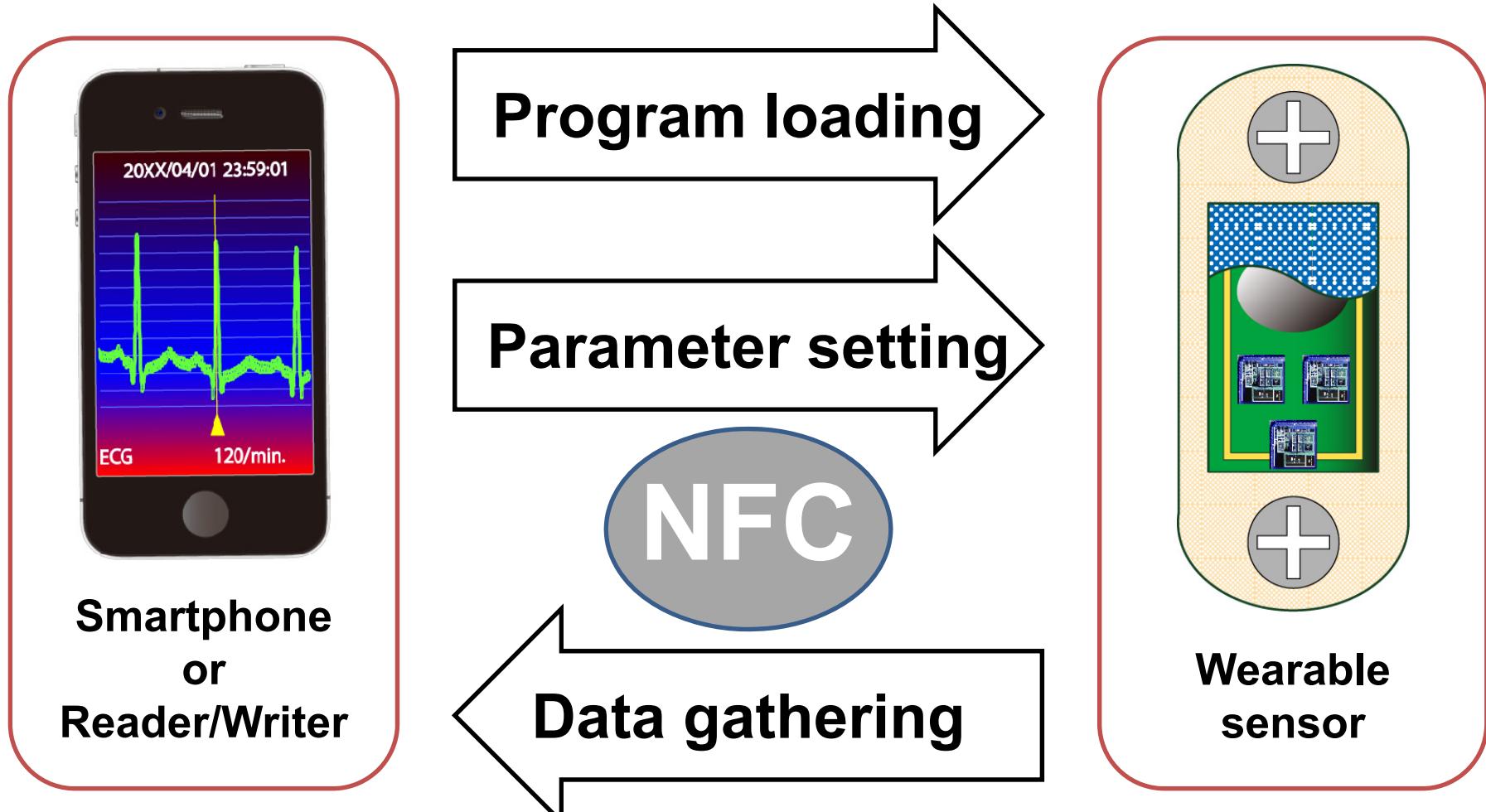


Problems:
Current consumption
(average, peak)
SNR degragation

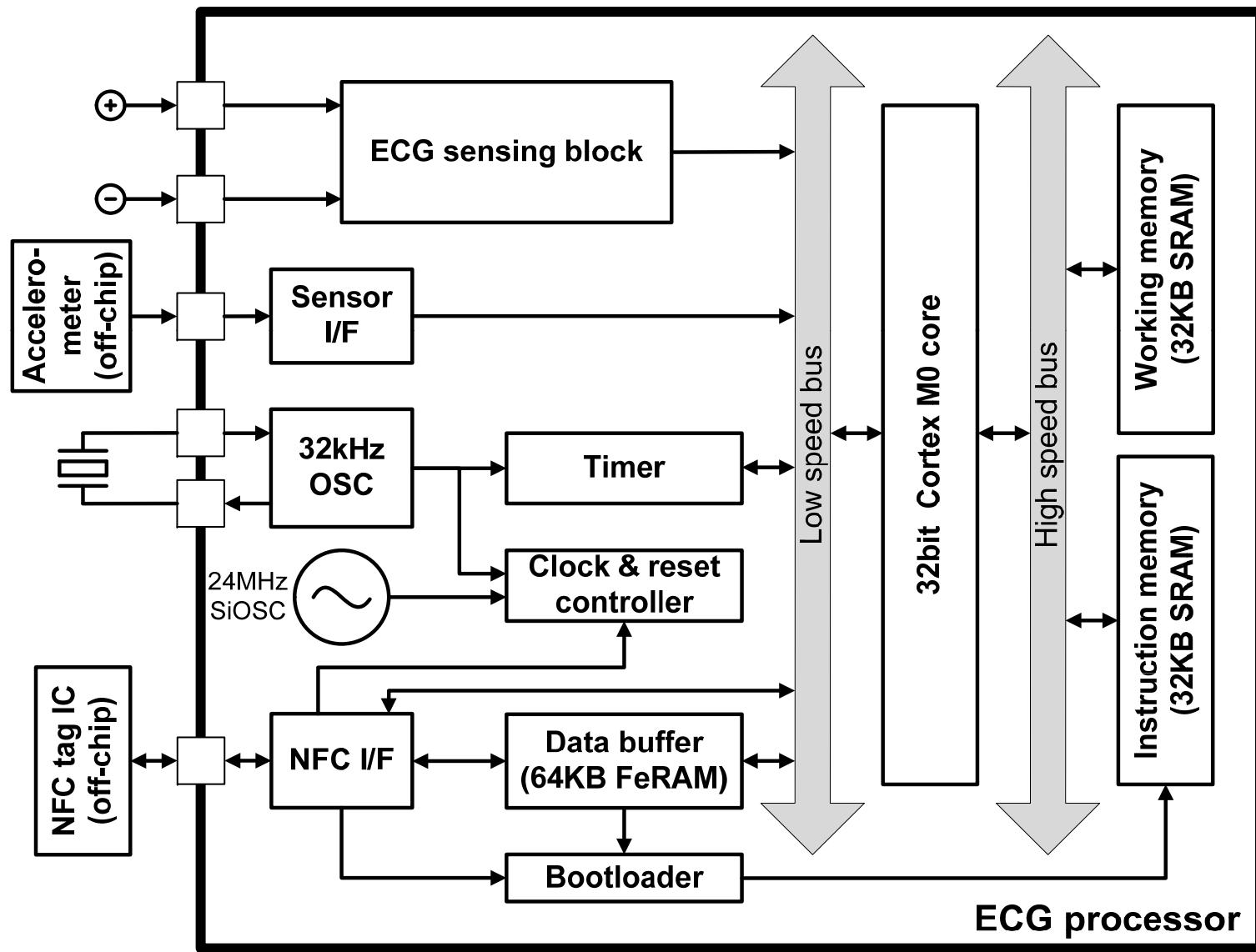
Normally-off strategy

- ❖ Wireless communication
 - Passive NFC (Near Field Communication)
- ❖ Leakage current of data buffer
 - FeRAM
- ❖ Active current of analog front end
 - Low-cost amplifier and ADC with noise tolerant algorithm

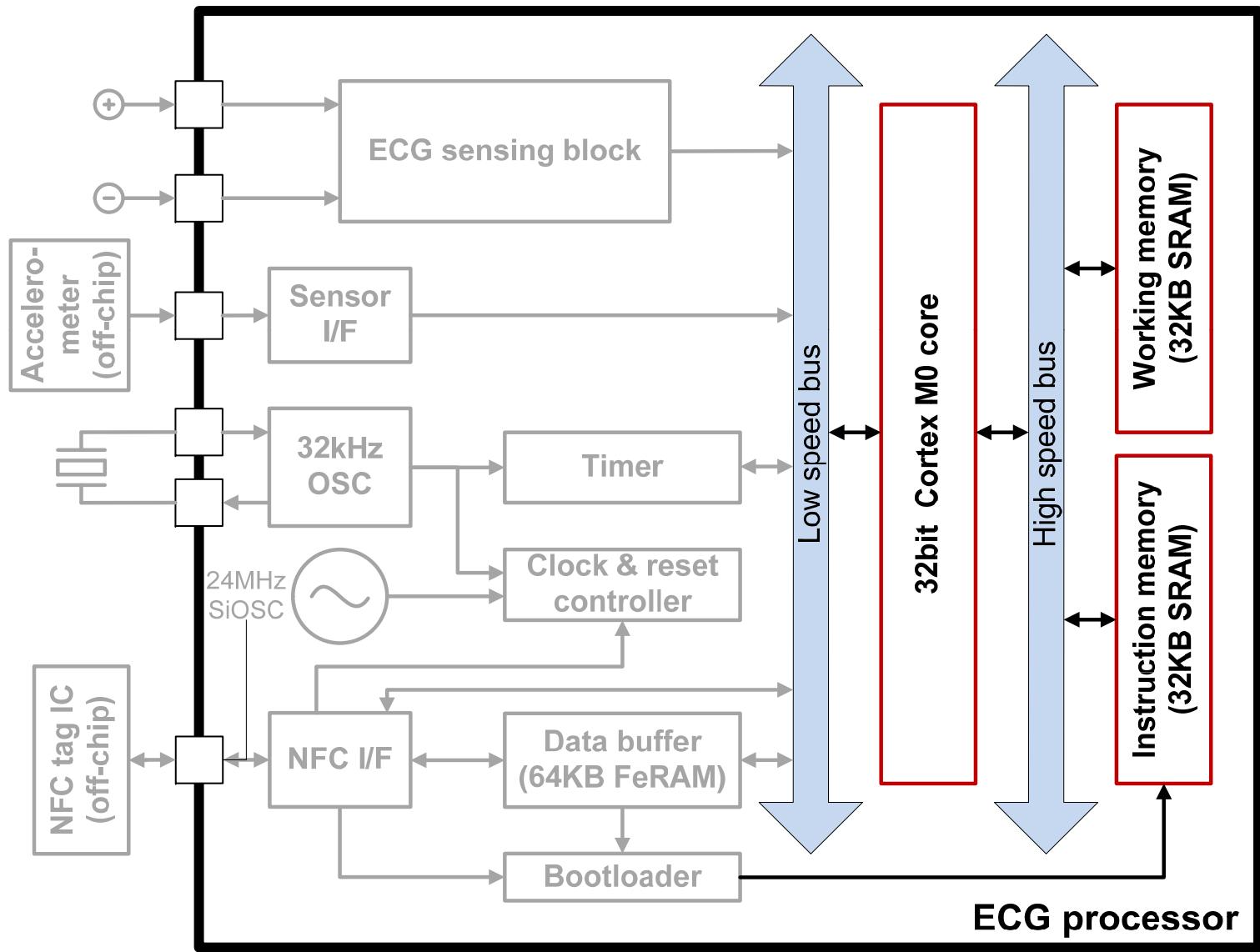
Passive NFC tag IC usage



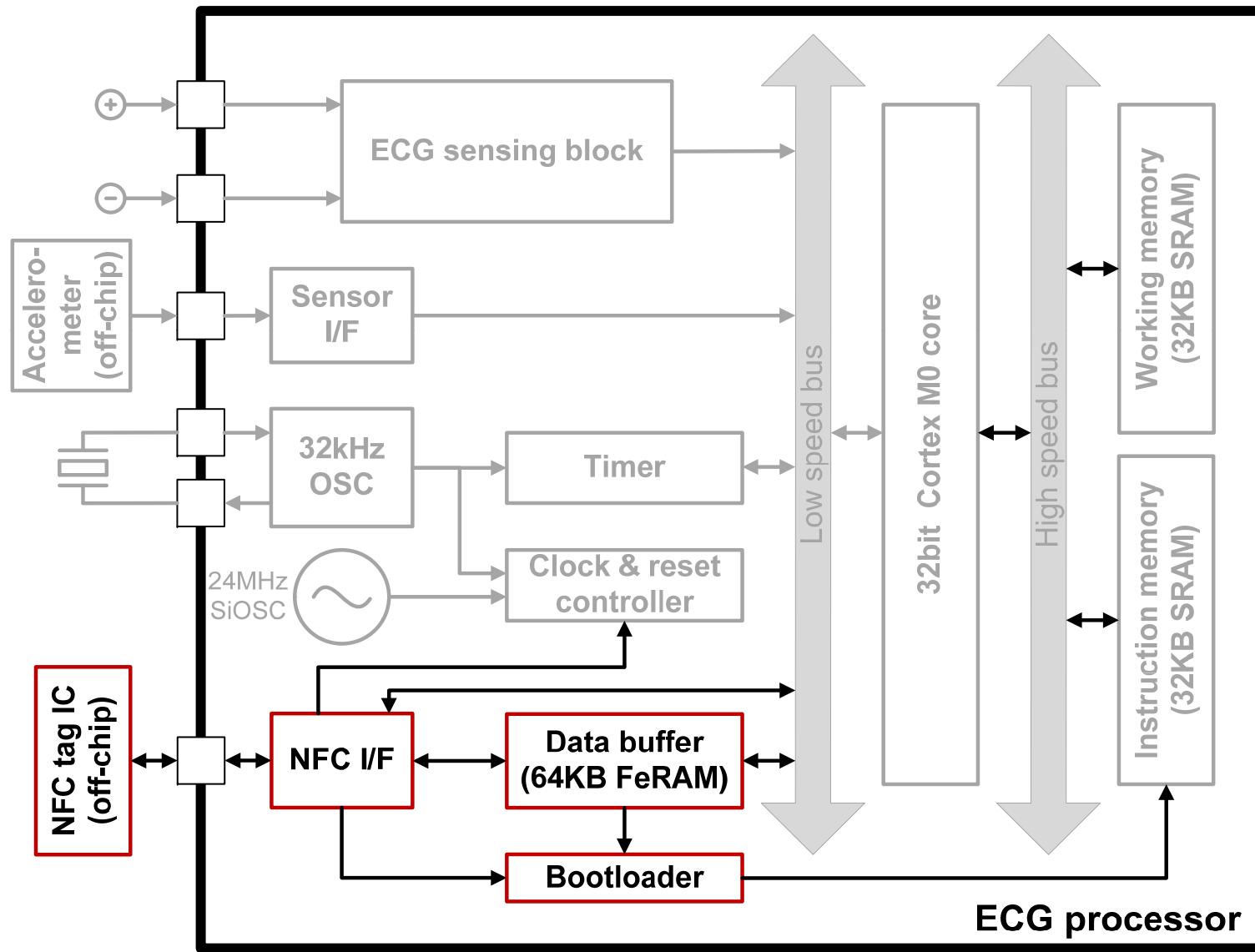
System Architecture



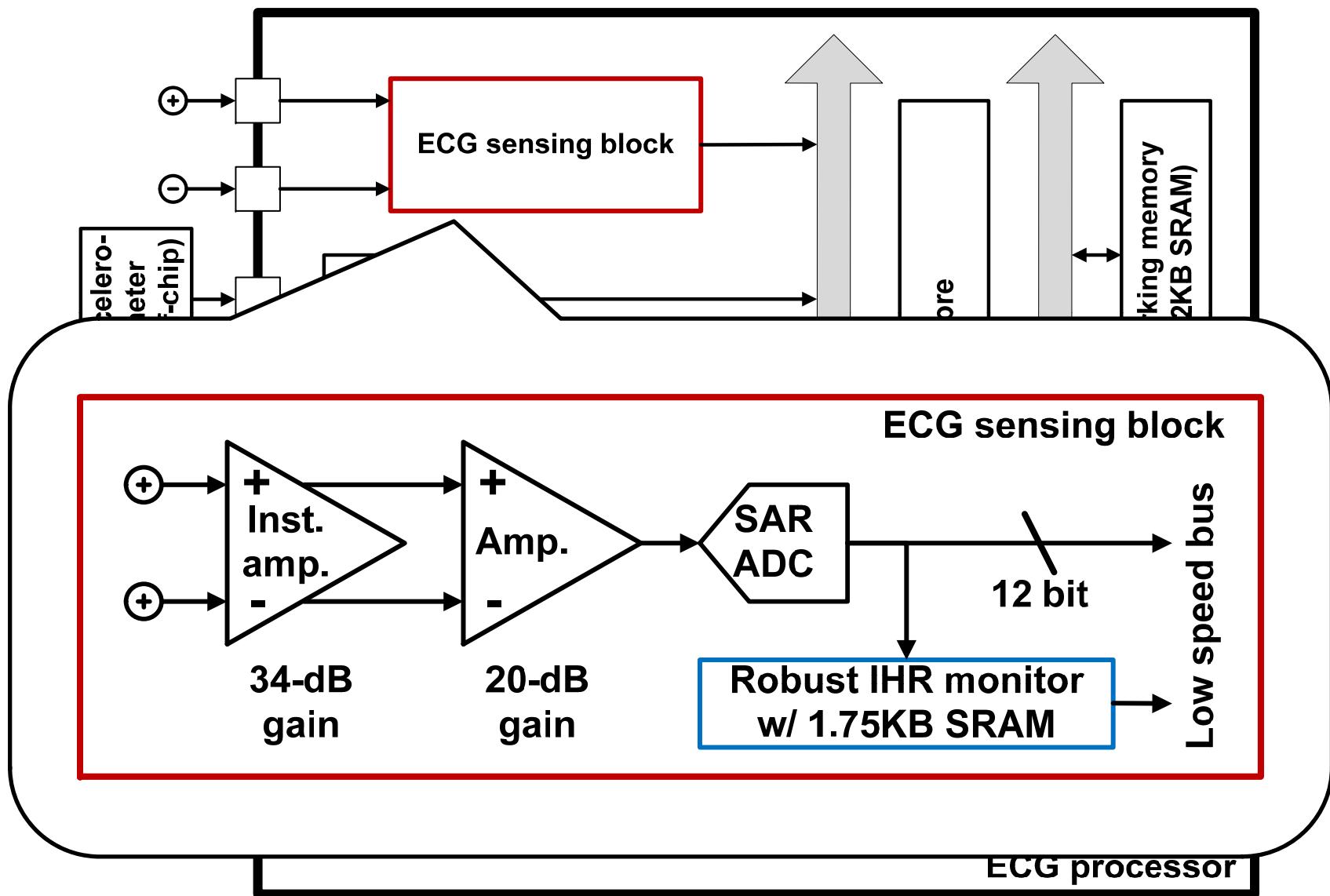
Cortex M0 core



Data Communication

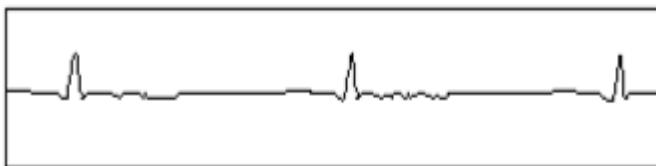


Robust IHR Monitor



Noises in wearable ECG

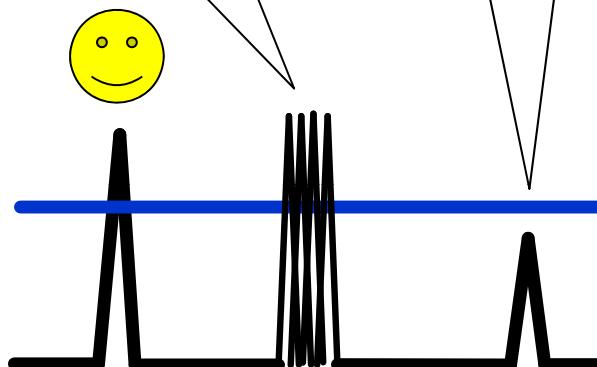
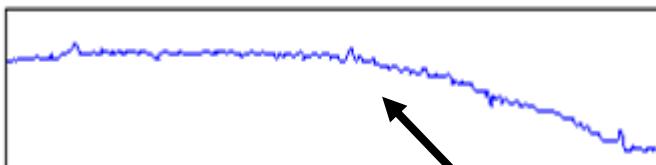
Clean ECG
(10~30Hz)



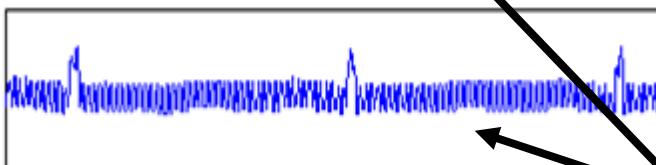
False Positive

False Negative

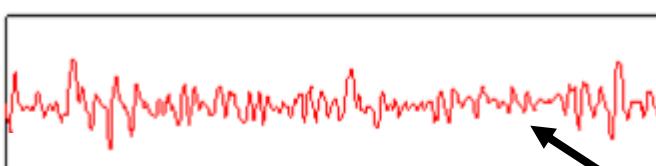
Baseline drift
(~3Hz)



Hum noise
(50,60Hz)

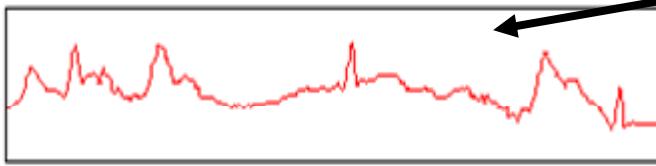


Muscle noise
(10~1kHz)



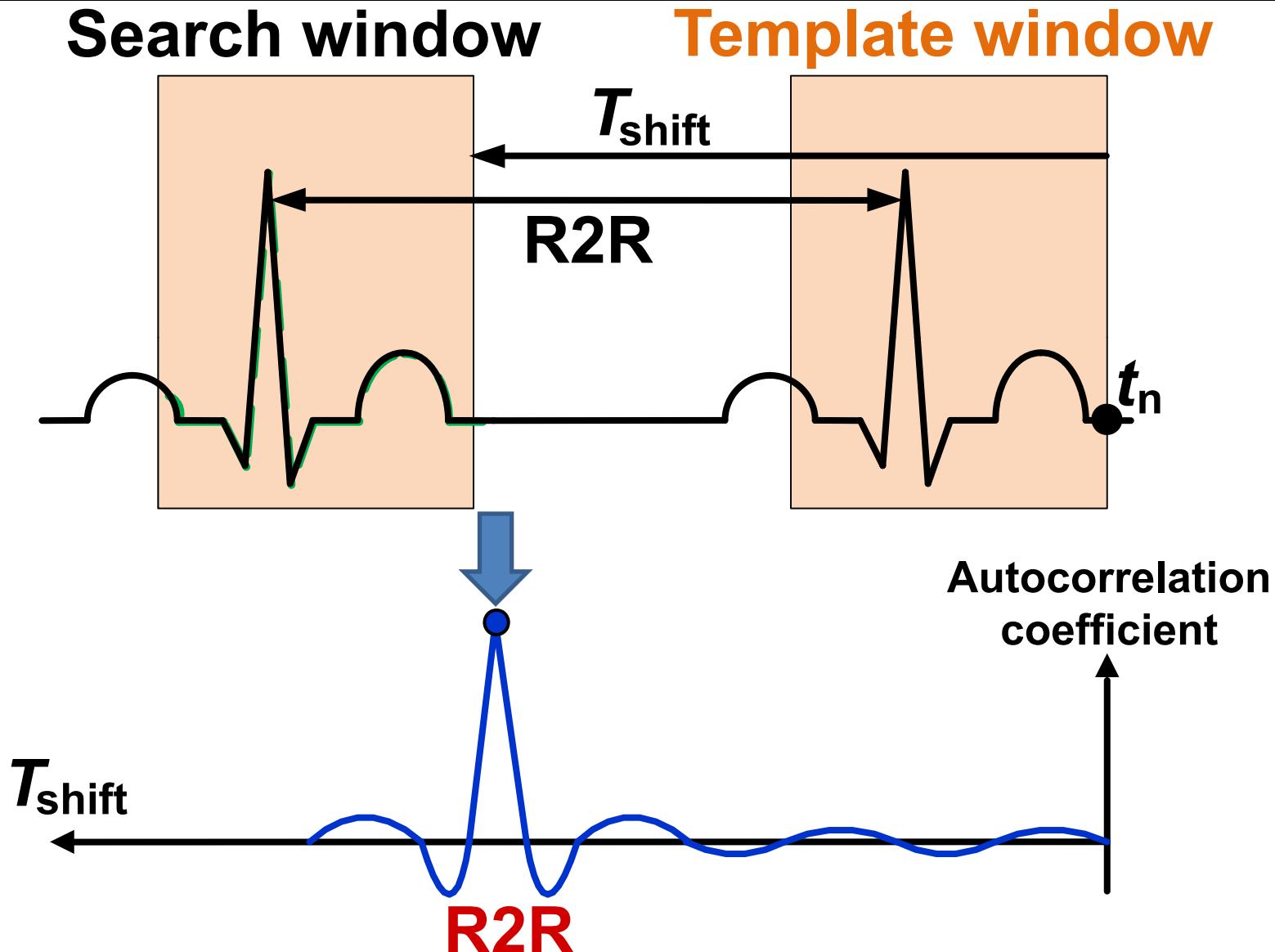
Removable

Motion artifact
(5~20Hz)



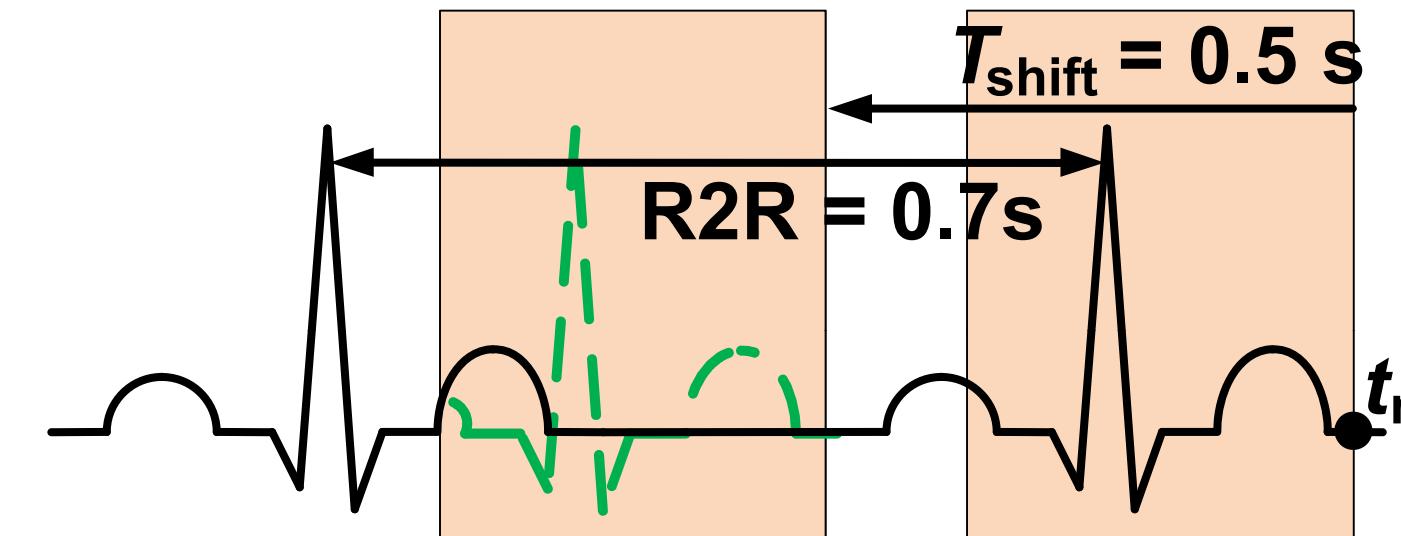
Difficult to remove

Short-Term Autocorrelation Algorithm



Short-Term Autocorrelation Algorithm

Search window

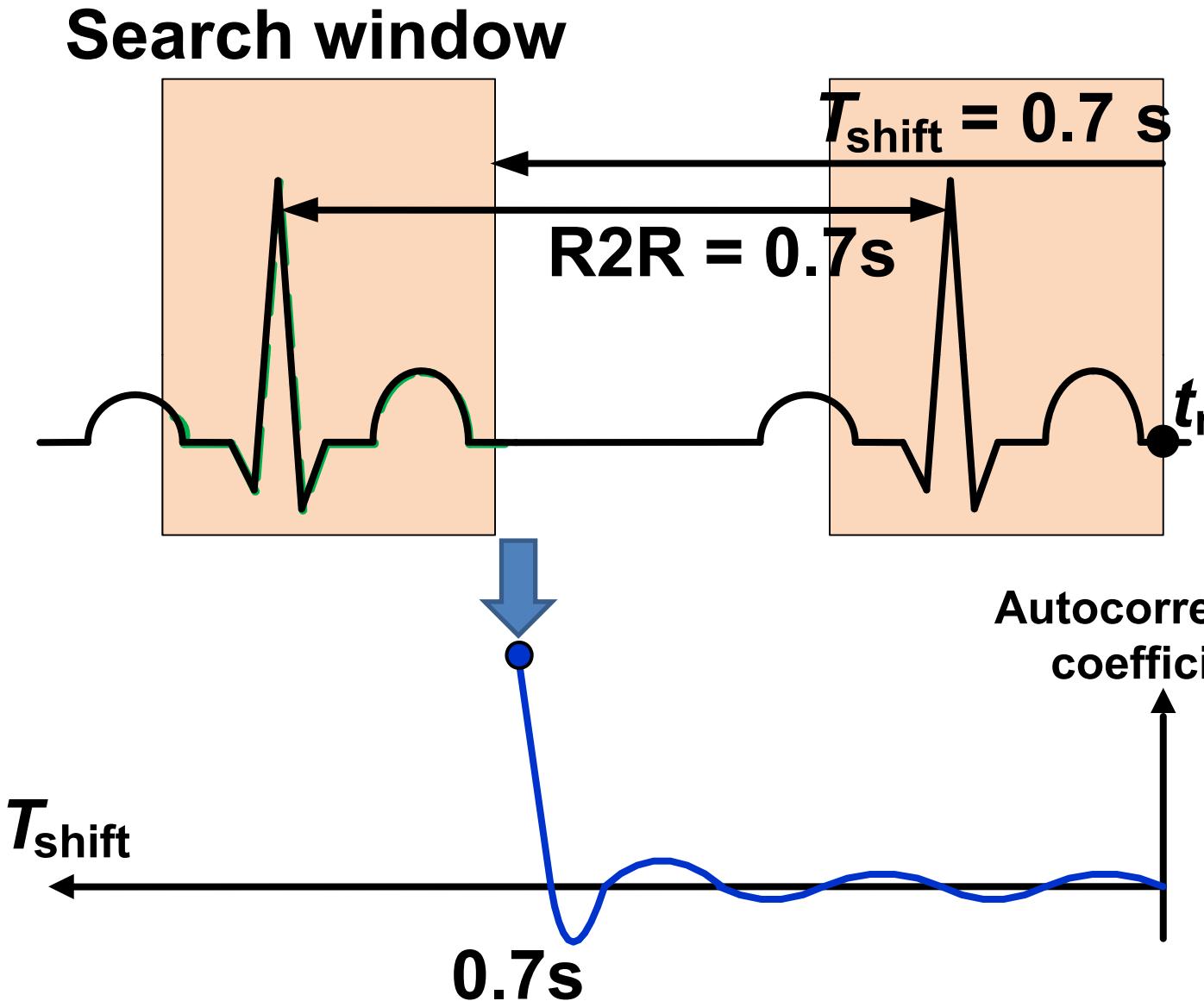


Autocorrelation
coefficient

T_{shift}

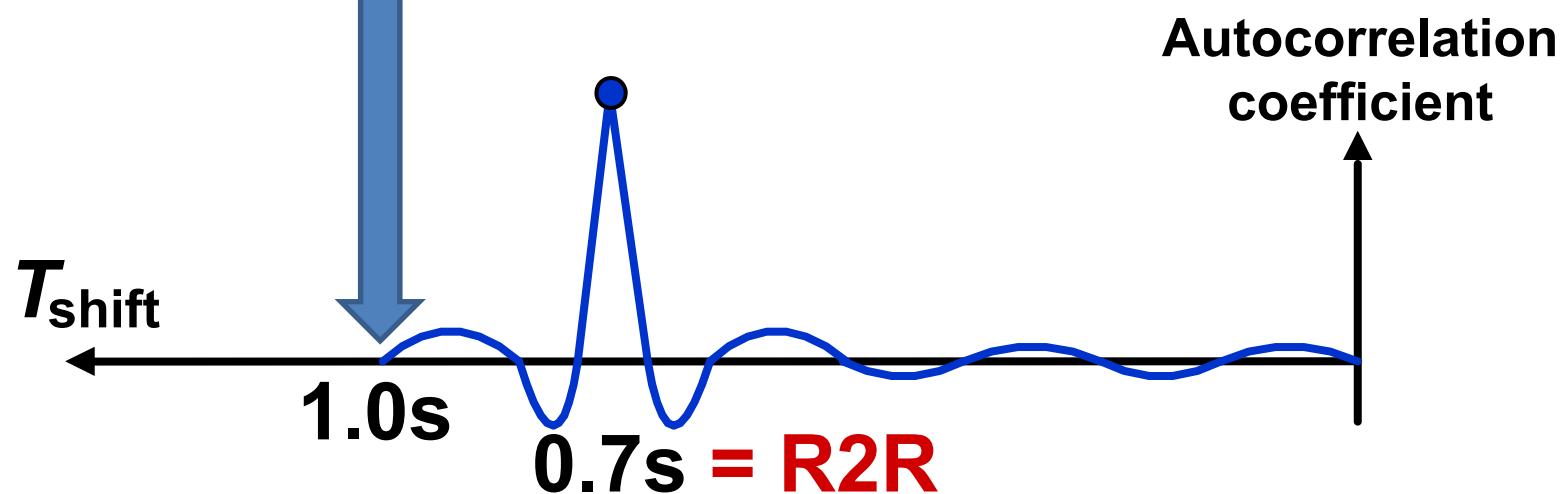
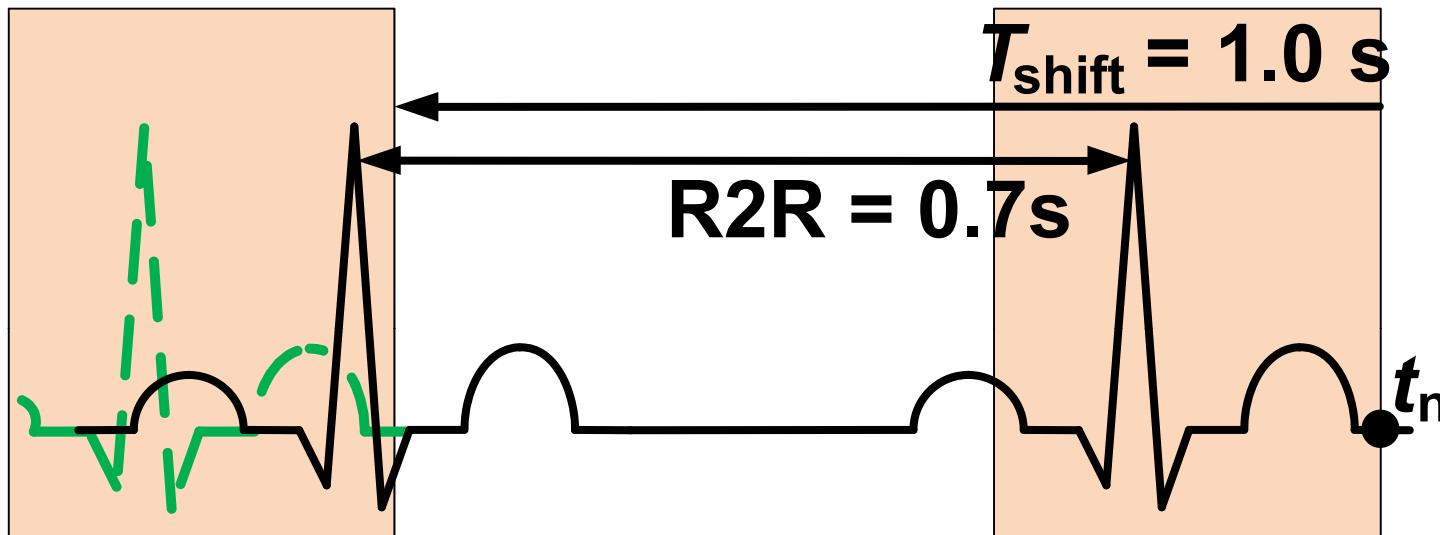
0.5s

Short-Term Autocorrelation Algorithm

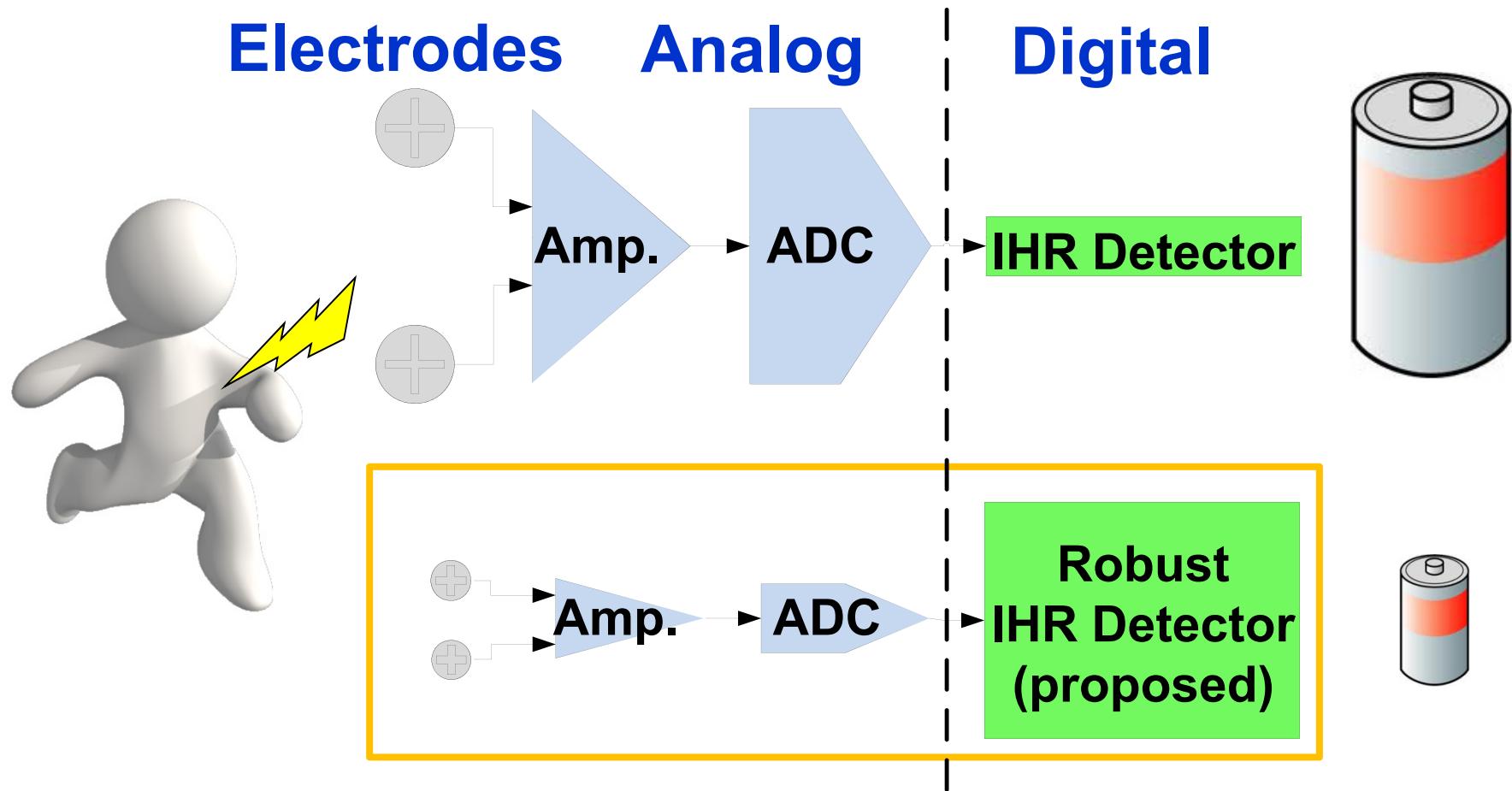


Short-Term Autocorrelation Algorithm

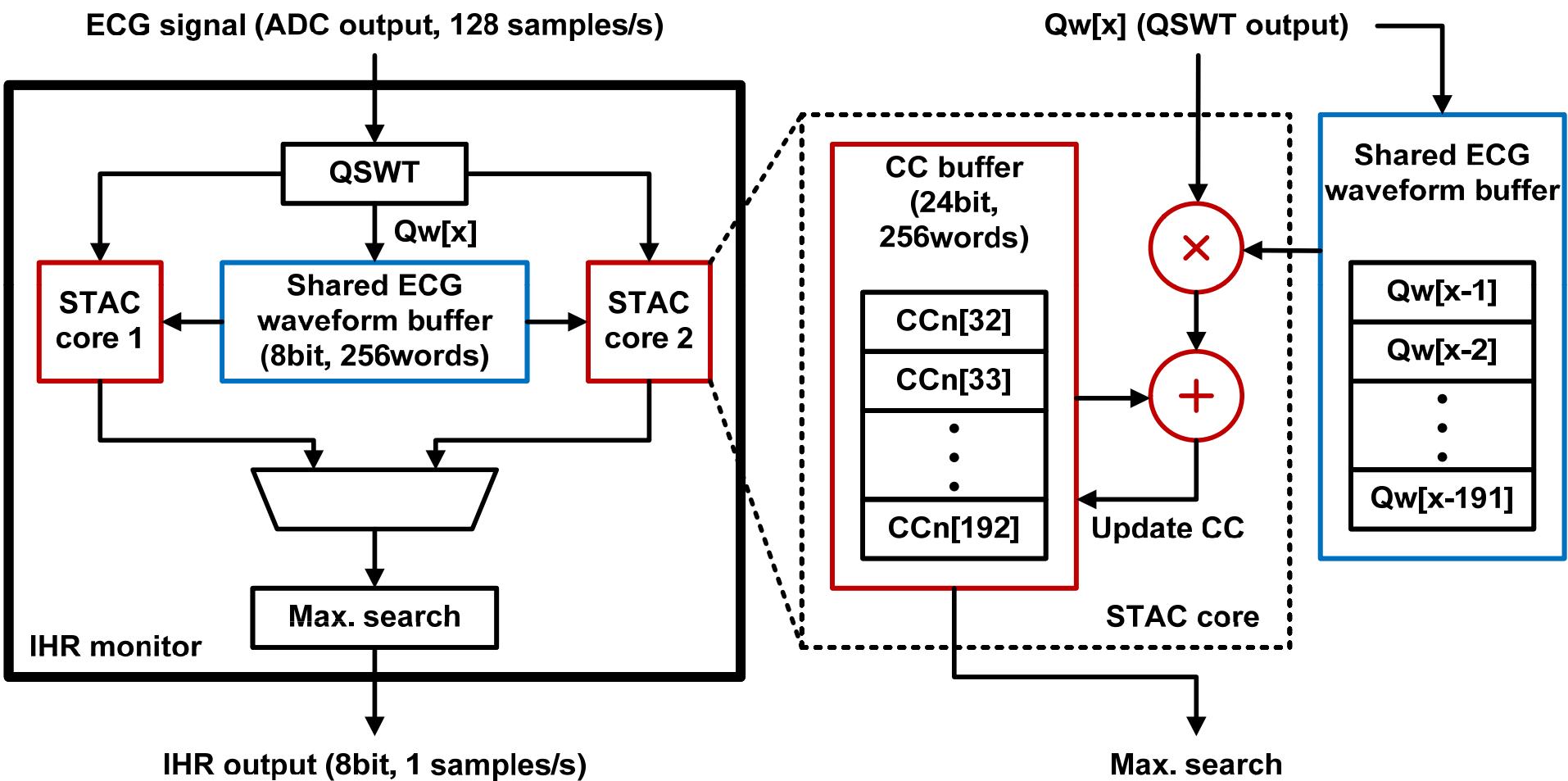
Search window



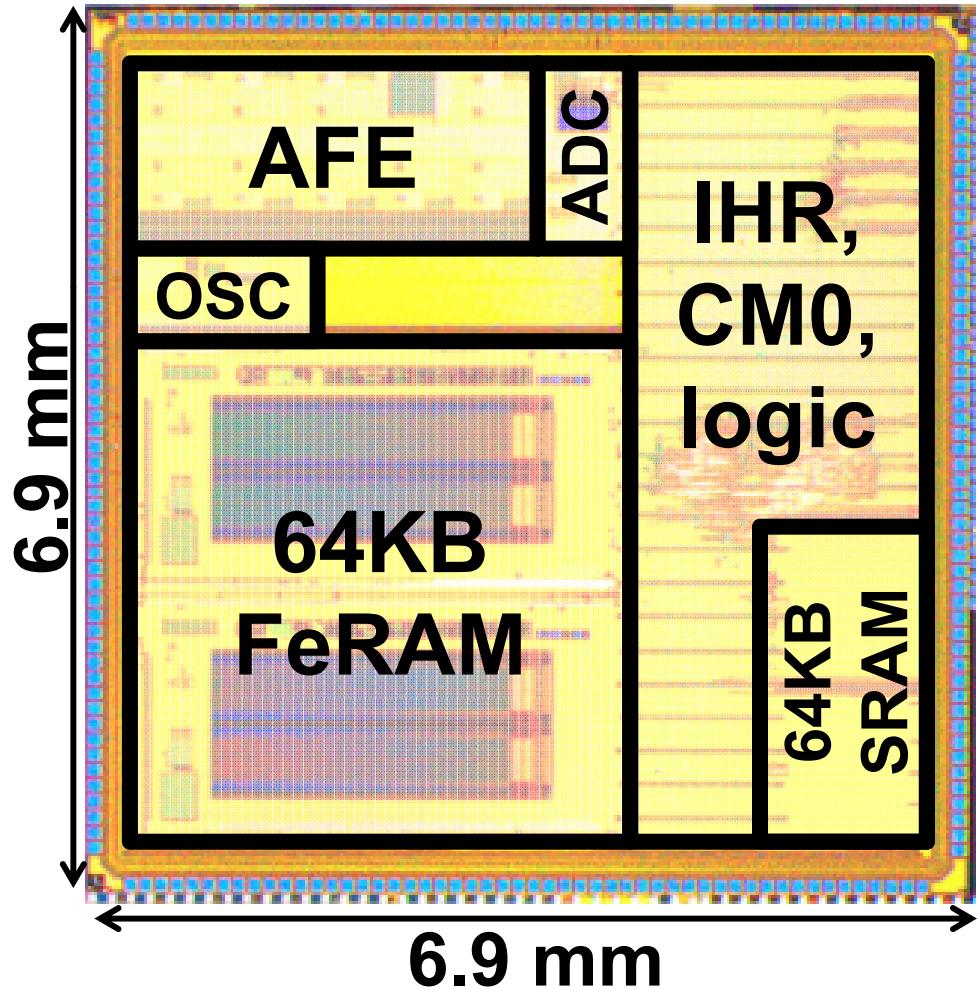
Our Approach for ECG Sensing



Architecture of IHR monitor

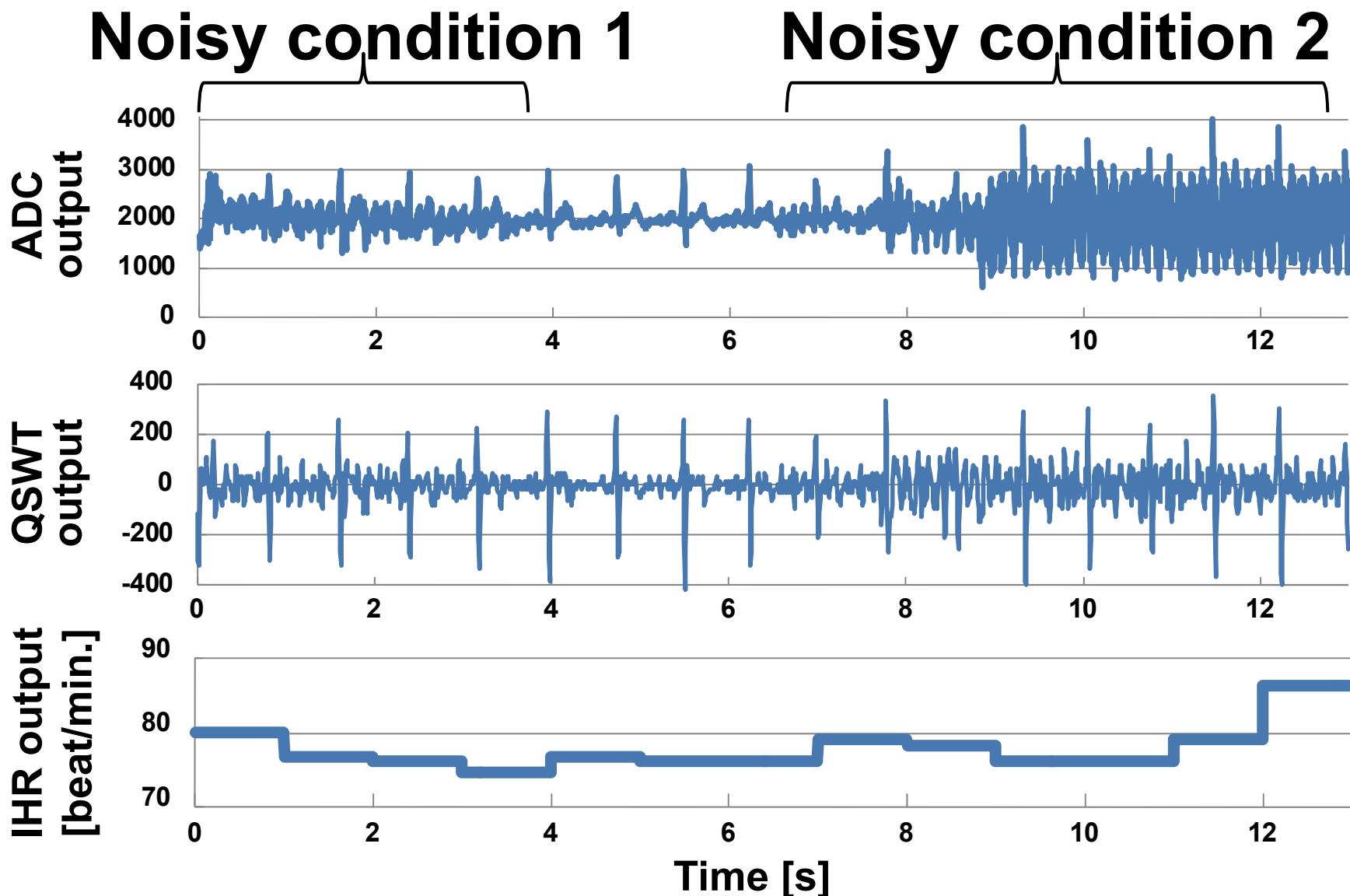


Die Micrograph and Specification

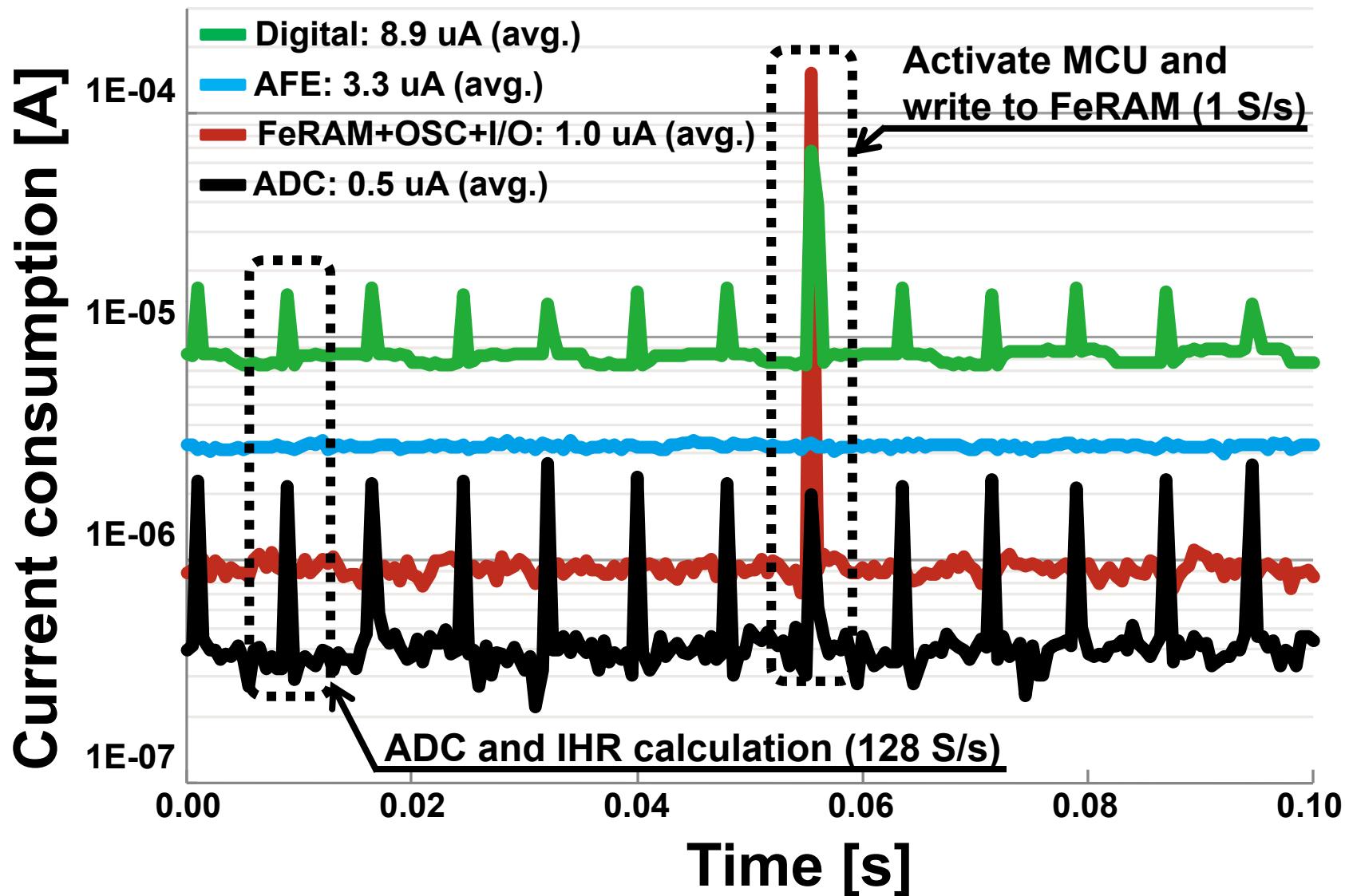


Technology	130-nm CMOS
Supply voltage	1.2V (Digital, SRAM, ADC, AFE)
	3.0V (FeRAM, 32kHz OSC, I/O)
Chip area	6.9 mm × 6.9 mm
Frequency	24 MHz (for MCU)
	32 kHz (for other blocks)
MCU	32-bit Cortex M0
On chip memory	64-KB FeRAM (for logging data)
	64-KB SRAM (for MCU)
	1.75-KB SRAM (for IHR detecto
ADC	Resolution 12 bit
	Current 0.5 μ A@128 S/s, 1.4 μ A@1 kS/s
AFE	Gain 54 dB
	Bandwidth 0-100 Hz
	Current 3.4 μ A
Total current 13.7 μ A (for heart rate logging)	

Measurement



Measurement



Comparison

	This work	ISSCC'12 [12]	VLSI'11 [13]
Technology	130 nm	130 nm	180 nm
Supply voltage	1.2V/3.0V	0.3-0.7V	1.2V
Frequency	24 MHz/32 kHz	1.7 MHz-2 kHz	1 MHz
MCU	Cortex M0 (32 bit)	8b RISC	n/a
On chip memory	129.75 kB	5.5 kB	46 kB
Total power for heart rate extraction	18.24 μ W	19 μ W	31.1 μ W
Total current for heart rate extraction	<u>13.7 μA</u>	>27 μ A	25.9 μ A

Conclusion

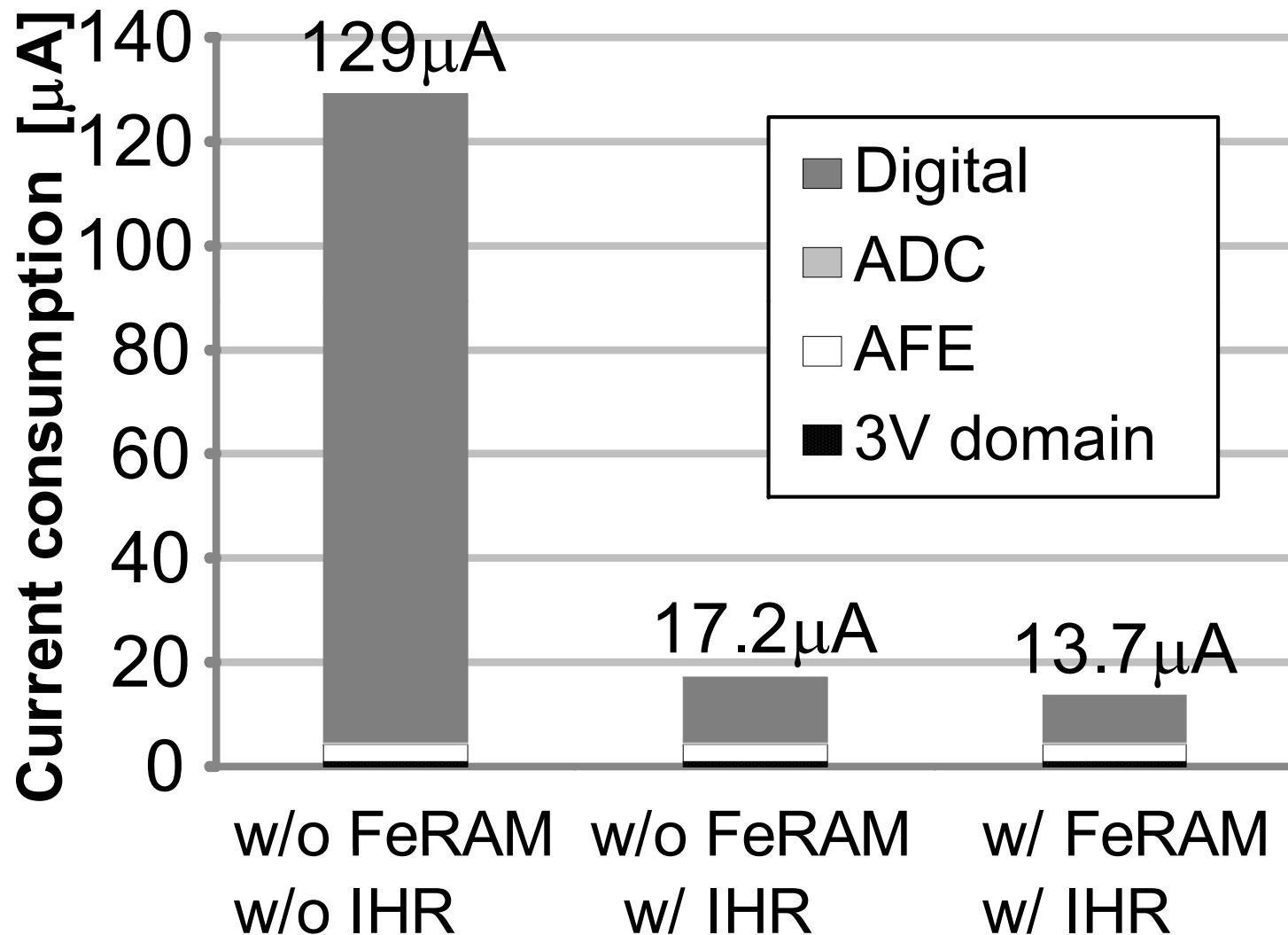
- ❖ The low-power wearable sensor using normally-off strategy was presented
- ❖ The noise tolerant ECG processor chip was fabricated in $0.13\mu\text{m}$ CMOS
- ❖ The robust IHR monitor using short-term autocorrelation algorithm consumes $1.21\mu\text{A}$
- ❖ The test chip totally consumes $13.7\mu\text{A}$ in IHR logging application

Acknowledgement

This research was supported by Ministry of Economy, Trade and Industry (METI) and the New Energy and Industrial Technology Development Organization (NEDO).

Thank you !

Performance Summary

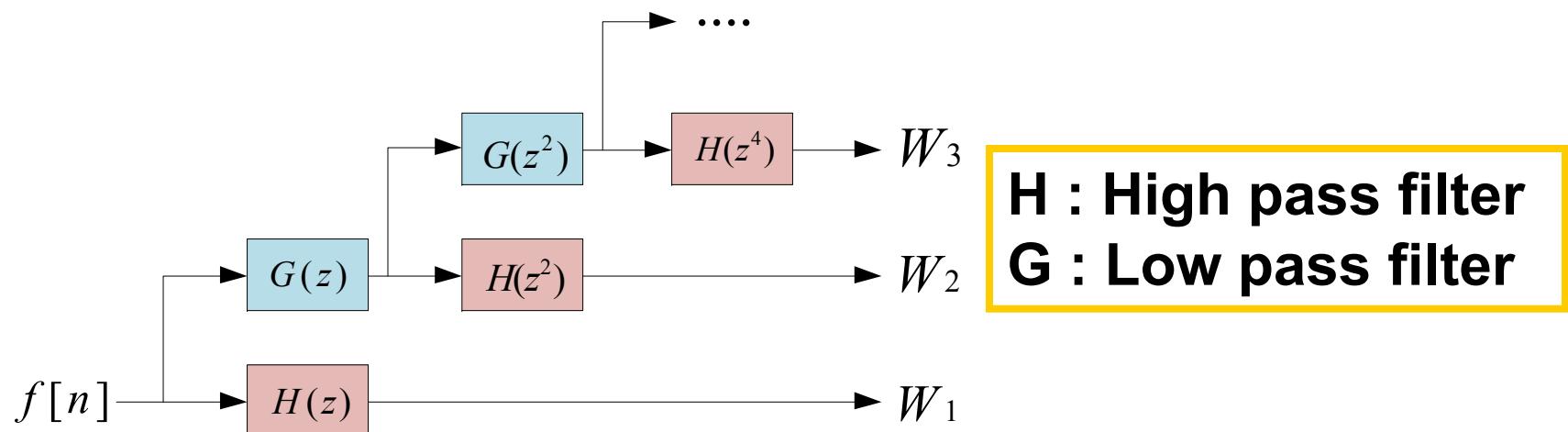


Wavelet Transform (WT)

- Both time and frequency analysis

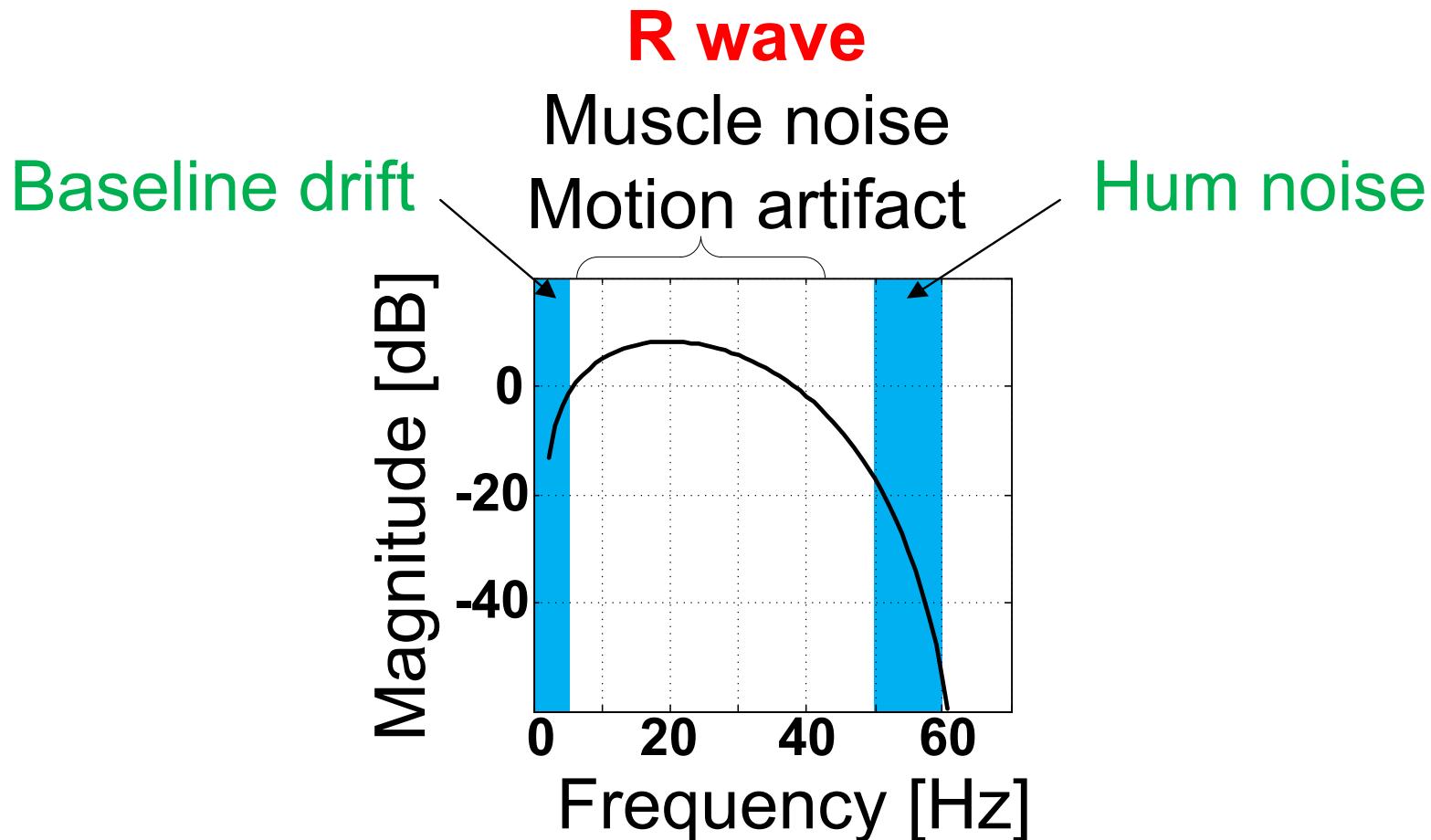
$$W_f(a, b) = \frac{1}{\sqrt{|a|}} \int_{-\infty}^{\infty} \overline{\psi\left(\frac{x-b}{a}\right)} f(x) dx$$

- ψ : mother wavelet
(decide a kind of transform)
- Discrete WT (DWT) consists of digital filters



Wavelet Transform

- Sampling frequency = 128Hz
- A kind of Band Pass Filter (BPF)



SNR

$$SNR = 10 \log \frac{S}{N \times a^2}$$

S : The peak-to-peak amplitude of QRS complex

N : Frequency-weighted noise power

a : Scale factor